

# LOW-POWER SILICON NEURONS, AXONS, AND SYNAPSES

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Power consumption is the dominant design issue for battery-powered electronic devices. Biologically-inspired sensory preprocessors may be an important component of portable computing devices that require real-world visual or auditory input. The silicon neural design style presented in (Mead, 1989; Andreou et al., 1991) naturally supports low-power VLSI design; in this design style, MOS transistors typically operate in the weak-inversion regime. The low-power performance of this design style is outstanding; for example, (Watts et al., 1991) reports on a 51-stage silicon cochlea, that computes all outputs in real time and consumes 11  $\mu$ W.

However, several popular circuits in this design style operate transistors outside the weak-inversion regime. These circuits, that model the spiking behavior of the axon hillock and the pulse propagation of axons, dominate power consumption in many neural chips (Lazzaro and Mead, 1989ab; Lazzaro, 1991; Horiuchi et al, 1991).

This chapter describes modified versions of these axon circuits. The modified circuits have been designed and fabricated and are fully functional; these circuits show a measured improvement in power consumption over the original circuits. Power consumption decreases of a factor of 10 to 1000 have been measured, depending on pulse width and spiking frequency. The density of the modified circuits is comparable to the original circuits. This chapter also describes several low-power synaptic circuits.

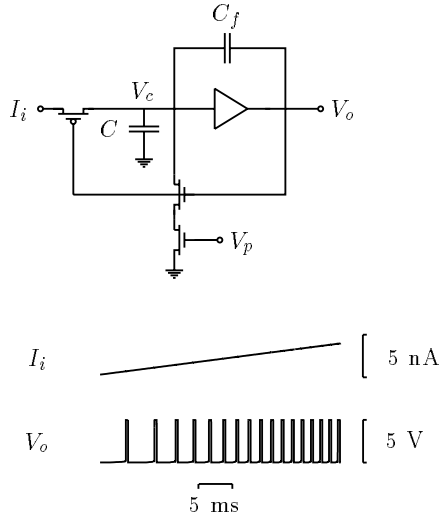
## AXONAL CIRCUITS

Figure 1 shows the spiking neuron circuit from (Mead, 1989), that uses a high-gain voltage amplifier with a sigmoidal nonlinearity as a gain element. The circuit converts the unidirectional current  $I_i$  into a sequence of fixed-width, fixed-height voltage pulses of  $V_o$ . During a pulse  $V_o = V_{dd}$ , and between pulses  $V_o$  is at ground potential.

To understand circuit operation, consider the circuit condition after an output pulse has completed. In this state,  $V_o$  is at ground potential, and  $V_c$  is lower than the switching threshold of the amplifier. The discharge path of the state capacitor  $C$  is closed, and the charging path of  $C$  is open.

The circuit remains in this state until the input current  $I_i$  increases  $V_c$  to the switching threshold of the amplifier. At this point,  $V_o$  switches to  $V_{dd}$ . The feedback capacitor  $C_f$  ensures the secure switching of the circuit. The new value of  $V_c$  is above the switching threshold of the amplifier, and depends on the relative values of  $C_f$  and  $C$ .

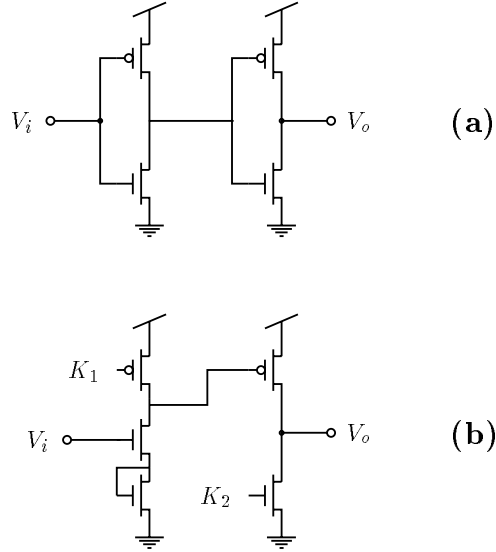
Once a pulse begins, the discharge path of the state capacitor  $C$  is open, and the charging path of  $C$  is closed. The control voltage  $V_p$  sets the discharge rate of  $C$ , and thus the width of voltage pulse of  $V_o$ . The circuit remains in this state until  $V_c$  decreases to the switching threshold of the amplifier. At this point,  $V_o$  switches to ground potential, and the pulse is complete. The voltage  $V_c$  is reset to a value below the switching threshold of the amplifier, that depends on the relative values of  $C_f$  and  $C$ .



**Figure 1.** Spiking neuron circuit and function, with unidirectional current input  $I_i$ , voltage pulse output  $V_o$ , and pulse width control voltage  $V_p$ .

This circuit, as described in (Mead, 1989), uses two digital inverters in series as the high-gain amplifier; Figure 2(a) shows this amplifier implementation. When used in the spiking neuron circuit, the transistors in first inverter of this amplifier are biased outside the weak-inversion regime. In many designs, the static current consumption of these transistors dominates the current consumption of the chip.

Figure 2(b) also shows a low-power implementation of a high-gain amplifier suitable for use in the spiking neuron circuit. The control voltages  $K_1$  and  $K_2$  limit the static current consumption of the amplifier. The response time of the amplifier is not symmetric; the speed of crossing the amplifier threshold in a positive direction is not limited by  $K_1$  and  $K_2$ , but the speed of crossing the threshold in a negative direction is directly dependent on  $K_1$  and  $K_2$ . In many applications, this asymmetry allows the bias currents of the amplifier to be set in the weak-inversion regime. The diode-connected transistor acts to raise the switching threshold of the amplifier.

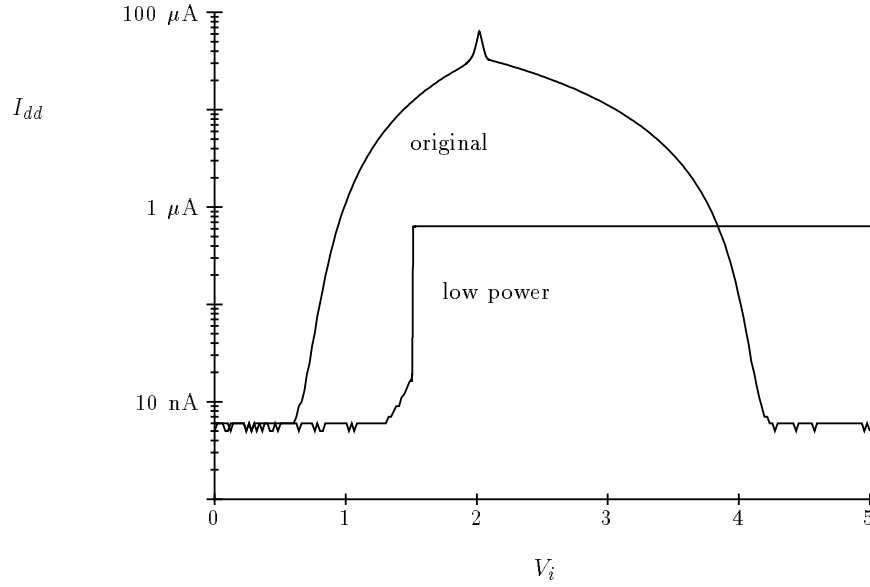


**Figure 2.** Original gain stage (a) and low-power gain stage (b).  $K_1$  and  $K_2$  are control voltages, set to ensure all transistors operate in the weak-inversion regime.

## AXONAL EXPERIMENTAL DATA

Figure 3 shows the static current consumption of the two amplifiers shown in Figure 2, as a function of the input voltage  $V_i$ . This figure shows data from a test chip fabricated in the  $2\mu\text{m}$  double polysilicon  $n$ -well Orbit process as supplied by MOSIS. The current meter used in this measurement is not able to measure currents below 5 nA. As expected, the low-power amplifier consumes negligible current below its switching threshold, and a constant current above its switching threshold.

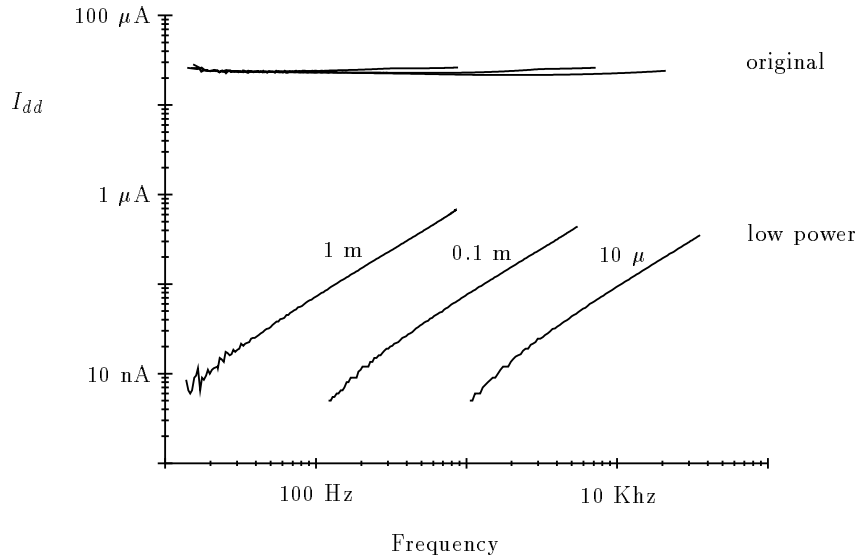
Figure 4 shows the current consumption of the spiking neuron circuit of Figure 1, implemented with the original amplifier and the low-power amplifier. As expected, the current consumption of the low-power circuit is a linear function of spiking frequency, and increases with the size of the pulse width. All data was taken with the values of  $K_1$  and  $K_2$  necessary for correct circuit function with  $10\mu\text{s}$  pulses; the current consumption for longer pulse-width operation can be reduced by adjusting  $K_1$  and  $K_2$ .



**Figure 3.** Power supply current  $I_{dd}$  for original gain stage and low-power gain stage, as a function of  $V_i$ . Note log scale for current.

## THE AXONAL DELAY CIRCUIT

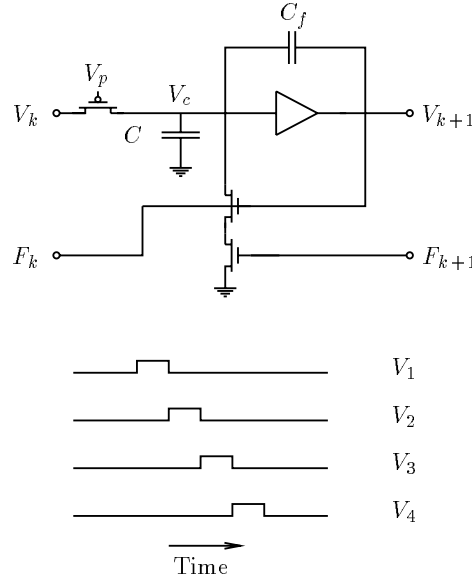
Figure 5 shows one section of the axonal delay line circuit described in (Mead, 1989). In engineering terms, the circuit is a cascade of non-retriggerable monostables, each with a voltage output  $V_k$ , that is either at  $V_{dd}$  or at ground potential. To understand circuit operation, consider the condition  $V_k = V_{dd}$ ,  $V_{k+1} = 0$ ,  $F_{k+1} = 0$ . In this case, the voltage  $V_c$  as shown in Figure 5 is below the switching threshold of the amplifier. The discharge path of the capacitor  $C$  is closed, and  $C$  is charged by a current set by the voltage  $V_k - V_p \equiv V_{dd} - V_p$ . When the voltage  $V_c$  increases to the switching threshold of the amplifier,  $V_{k+1}$  changes to  $V_{dd}$ , and the axon stage associated with  $V_{k+2}$  begins a similar charging cycle. Once this cycle has completed, the voltage  $F_{k+1}$  switches to  $V_{dd}$  and the capacitor  $C$  associated with  $V_{k+1}$  quickly discharges, causing the voltage  $V_{k+1}$  to switch back to ground. In this way, a constant width voltage pulse propagates down the structure.



**Figure 4.** Power supply current  $I_{dd}$  for original spiking neuron circuit and low-power spiking neuron circuit, as a function of spiking frequency. Labels next to graphs indicate pulse width of spikes, in units of seconds. Note log scale for frequency and current.

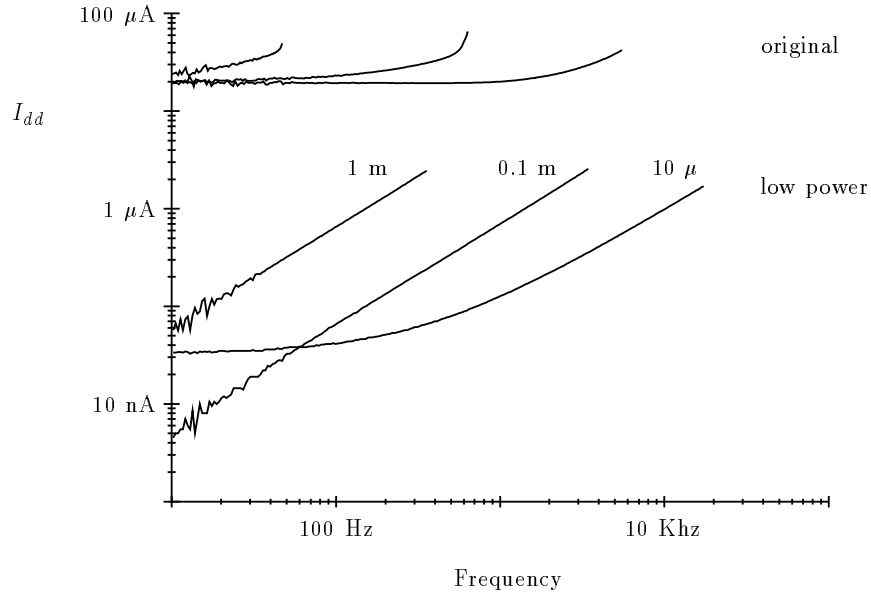
As with the spiking neuron circuit, the amplifier in each neuron circuit, if implemented with two digital inverters in series, consumes appreciable static current. Replacing the original amplifier with the low-power amplifier reduces the current consumption of an axonal delay circuit. Figure 6 shows the current consumption of an 18-stage axonal delay circuit, implemented with the original amplifier and the low-power amplifier.

For pulse widths of  $100\ \mu\text{s}$  and  $1\ \text{ms}$ , current consumption of the low-power axon circuit is a linear function of spiking frequency. For a pulse width of  $10\ \mu\text{s}$ , the state capacitors  $C$  are not fully discharged with a single pulse, and some additional static current consumption occurs. As with the spiking neuron circuit, the current consumption of the low-power axon circuit also depends on pulse width length. All data was taken with the values of  $K_1$  and  $K_2$  necessary for correct circuit function with  $10\ \mu\text{s}$  pulses; the current consumption for longer pulse width operation can be reduced by adjusting  $K_1$  and  $K_2$ .



**Figure 5.** Axon circuit and function. Labels include ports  $V_k$  and  $F_k$  to previous stage, ports  $V_{k+1}$  and  $F_{k+1}$  to next stage, pulse width control voltage  $V_p$ , state voltage  $V_c$ , state capacitor  $C$  and feedback capacitor  $C_f$ .

The original axon circuit has a single free parameter,  $V_p$ , that sets both the speed of pulse propagation and the width of each pulse. The low-power axon circuit provides two additional parameters,  $K_1$  and  $K_2$ . These parameters permit the pulse width and propagation speed to be set independently, allowing overlapping pulses in successive taps.



**Figure 6.** Power supply current  $I_{dd}$  for original axon circuit and low-power axon circuit, as a function of spiking frequency (18 sections). Labels next to graphs indicate pulse width of spikes, in seconds. Note log scales for current and frequency.

## SYNAPTIC CIRCUITS

This section describes several different types of low-power synaptic circuits. Referring to Figure 1, synaptic circuits convert the pulse output representation of the signal  $V_o$  into a unidirectional weak-inversion current signal suitable for connection in  $I_i$ . Different synaptic circuits perform different types of signal processing during the conversion. All of the circuits in this section have been fabricated as components in functional systems, except where indicated.

Figure 7 shows simple synaptic circuits. The circuit in Figure 7(a) (Mead, 1989) is a very simple synapse, converting a downward voltage pulse into the unidirectional current output  $I_o$ . The magnitude of the current pulse is set by

the control voltage  $V_w$ , and the width of the current pulse reflects the width of the input voltage pulse.

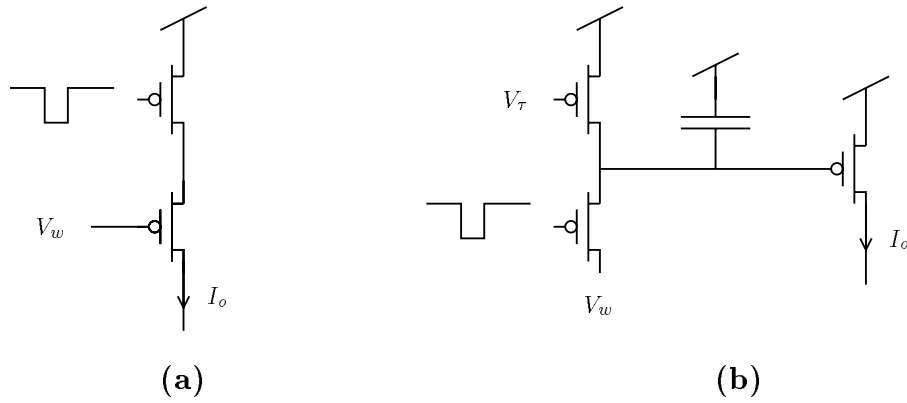
In some situations, the width of the input voltage pulse is very small and not under voltage control; in particular, pulse outputs from spiking neuron circuits used in off-chip communication have this property. (Lazzaro et al., 1993). The synapse circuit shown in Figure 7(b) is designed to produce an output current pulse  $I_o$  that is wider than the input voltage pulse. The control voltage  $V_r$  sets the width of  $I_o$ , and the control voltage  $V_w$  sets the magnitude.

The circuits in Figure 7 allows voltage pulses to be multiplied by a weight set by  $V_w$ , and summed together using Kirchoff's current law. Circuits shown in Figure 8 are useful for performing signal processing on this aggregate current signal. These circuits transform a unidirectional input current  $I_i$  into a unidirectional output current  $I_o$ .

The circuit in Figure 8(a) includes two control voltages,  $V_1$  and  $V_2$ , which can be used together to scale  $I_i$  by factors greater than or less than unity. If all transistors are operating in the weak-inversion regime, the equation

$$I_o = I_i e^{(\kappa/2)(V_1 - V_2)/V_o}$$

describes the operation of the circuit, where  $V_o = kT/q$  and  $\kappa$  is a fabrication constant as described in (Mead, 1989).



**Figure 7.** Synapses circuits, producing output currents  $I_o$ .



The circuit in Figure 8(b) is similar to the circuit in Figure 8(a), but uses the currents  $I_1$  and  $I_2$  to scale the input current. If all transistors are operating in the weak-inversion regime, the equation

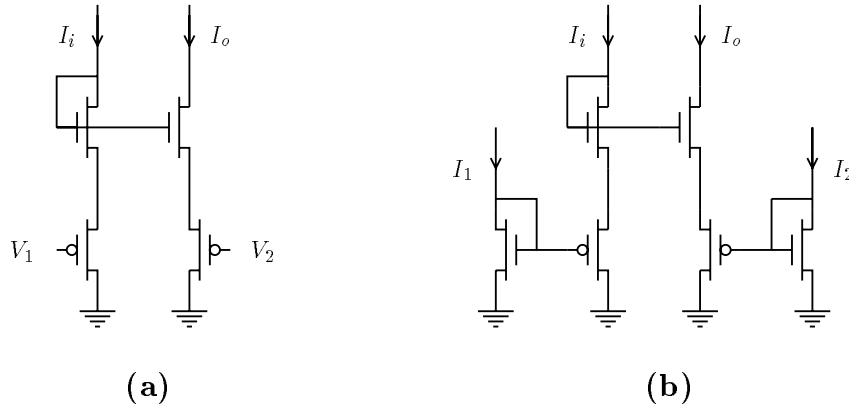
$$I_o = I_i \sqrt{I_1/I_2}$$

describes the operation of the circuit.

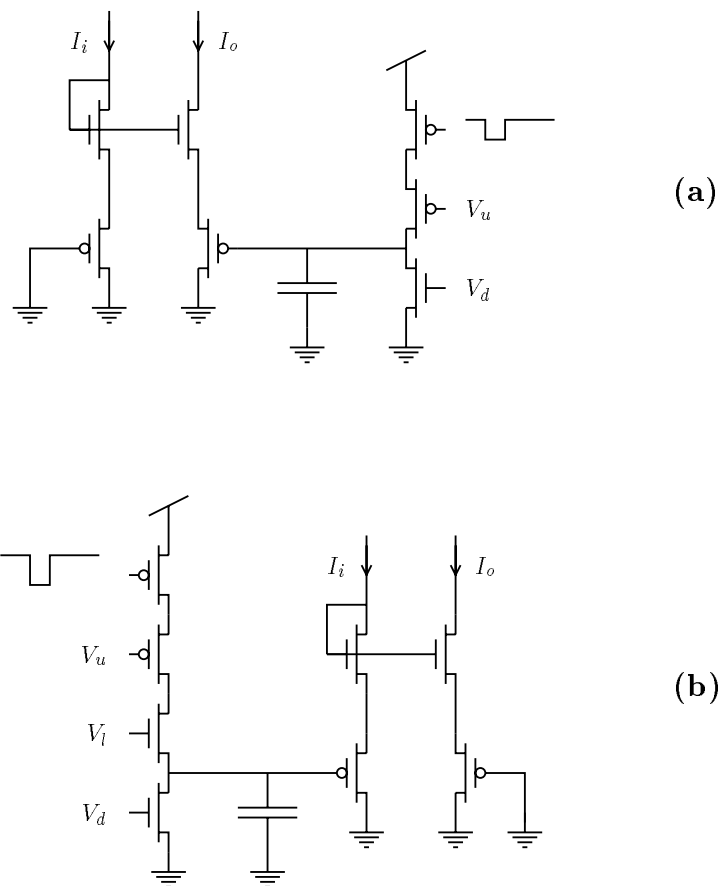
The scaling circuits of Figure 8 can be used as components for circuits that implement adaptation or facilitation. Figure 9(a) shows an adaptation circuit, that has been used in an auditory nerve model (Lazzaro, 1992). The primary input of this circuit is  $I_i$ , a current usually obtained by summing the response of many simple synapses. The output of the circuit,  $I_o$ , is a scaled version of  $I_i$ . If the auxiliary input of this circuit (marked with a pulse) is inactive for an extended period of time, the circuit performs unity scaling. If the auxiliary input is active, however, the output  $I_o$  is a reduced version of  $I_i$ . The temporal characteristics of the adaptation are set by the control voltages  $V_u$  and  $V_d$ ; depending on the values of these parameters, the circuit can produce time constants as long as several seconds.

Figure 9(b) shows a facilitation circuit that operates on a similar principal to the adaptation circuit of Figure 9(a). In this circuit, auxiliary input activity scales  $I_o$  to be larger than  $I_i$ ; a lack of auxiliary input activity performs unity scaling. An additional control voltage,  $V_i$ , limits the maximum scaling of the circuit. This circuit simulates correctly but has not been used in a fabricated system.

The circuits in Figure 9 are both controlled by a single auxiliary input. This input can be replaced by a logical combination of several inputs, to produce a circuit suitable for learning algorithms.



**Figure 8.** Scaling circuits for currents:  $I_o = I_i \alpha(I_1, I_2, V_1, V_2)$ .



**Figure 9.** Short-term adaptation and facilitation circuits.

## CONCLUSIONS

This chapter reviews low-power circuit technology for spiking neurons, axons, and synaptic circuits. Using the circuits from this chapter, the reader should be able to recast many of the circuits from other chapters of this book into low-power designs.

## Acknowledgements

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